BETAMETHASONE PHARMACOKINETICS AFTER TWO PRODRUG FORMULATIONS IN SHEEP: IMPLICATIONS FOR ANTENATAL CORTICOSTEROID USE.

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d) Abbreviations: QC, quality control; $-_{BMp}$, $-_{BMa}$ and $-_{BMp/a}$, phosphate prodrug, acetate prodrug and dual phosphate/acetate formulation related variables; $C_{BMp}$ and $C_{BMp/a}$, betamethasone concentrations; $ka_{BMp}$ and $ka_{BMa}$, hybrid first-order rate constants; $Dose_{BMp}$ and $Dose_{BMa}$, doses of prodrugs in terms of betamethasone equivalents; $Vc/F_{BMp}$ and $Vc/F_{BMa}$, apparent volumes of distribution; $k_{el}$, elimination rate constant; $t_{1/2}$, half life; $F_{BMa}$ and $F_{BMp}$, bioavailability terms; $F_{BMp}/F_{BMp}$, relative bioavailability; $Y(t)$, model output function; $IC_{50,Free}$, free drug level causing 50% inhibition of cortisol synthesis rate; ADME, absorption, distribution, metabolism and excretion; CV%, Coefficient of Variation; HPLC, high-performance liquid chromatography; LC/MS/MS, liquid chromatography tandem mass spectrometry
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ABSTRACT:

Objective. Maternal administration of betamethasone to enhance fetal lung maturation for women who threaten preterm labor is common clinical practice. However, recommendations regarding the choice of betamethasone formulations for perinatal use are vague. The disposition of betamethasone from two commonly used antenatal formulations is poorly understood. We therefore designed a study to capture the true pharmacokinetic profiles of betamethasone from these fast acting and dual release formulations. Methods. Betamethasone in sheep plasma was measured by a newly designed highly sensitive liquid chromatography tandem mass spectrometry assay after intramuscular injection (n = 4) of 0.25 mg/kg of betamethasone phosphate and 0.5 mg/kg betamethasone phosphate/acetate formulations. Compartmental modeling was performed using the ADAPT II program. Results. Betamethasone pharmacokinetics could be captured for 24 hours for the phosphate and for 5 days for the phosphate/acetate formulations. The phosphate formulation profile appeared like a traditional Bateman function with a terminal half-life of 4 hours whereas the phosphate/acetate formulation produced a biexponential decline with a terminal half-life of 14 hours. The latter is much longer than commonly reported and has been missed in the literature due to assay limitations. Extrapolations to humans indicate that although both formulations might have similar therapeutic indices, the dual formulation might be associated with a lower safety profile. Conclusion. In light of this newly identified long terminal half-life for the betamethasone dual formulation, dosing practices for betamethasone in pregnancy need to be reassessed.
Preterm birth occurs in about 10% of pregnancies and complications associated with prematurity, especially respiratory distress syndrome, are the leading cause of mortality in prematurely born infants (NIH Consensus Panel, 1995). Betamethasone is administered maternally to enhance fetal lung maturation in women who threaten preterm labor during 24-34 weeks gestation. The NIH recommends administration of two maternal intramuscular injections of 12-mg betamethasone 24 hours apart for this condition. Although the doses of betamethasone are stated, the exact formulation recommendation is not clear. Betamethasone is available as a fast releasing phosphate ester prodrug formulation and as a dual acting suspension formulation containing phosphate and acetate ester prodrugs. Both formulations have been tested in clinical trials and have been shown to be efficacious in producing precocious fetal lung maturation (Liggins and Howie, 1972; Gamsu et al., 1989). However, there is controversy regarding the betamethasone releasing properties of the acetate prodrug and a recent meta-analysis suggests that this prodrug is probably of little therapeutic benefit for antenatal use (Jobe and Soll, 2004). Although the release properties of the acetate prodrug have been questioned, long duration studies looking at the release pattern of betamethasone from this prodrug do not exist. Furthermore, traditional chromatographic assays for betamethasone in animal studies suffer from sensitivity and sample stability issues that were raised in a recent meta-analysis (Samtani et al., 2004a). These problems remain unresolved and we therefore designed a study to capture the true pharmacokinetic profiles of betamethasone from the two formulations. The study design and rationale were as follows: a) The most commonly utilized animal model for fetal maturation studies is the pregnant sheep (Dunlop et al., 1997) and hence the pharmacokinetic investigation was
conducted in ewes. b) The formulations were compared in non-pregnant animals. Our meta-analysis (Samtani et al., 2004a) has pointed out that complete pharmacokinetic characterization of drugs in pregnancy requires complicated study designs involving maternal/fetal dosing and sampling. Corticosteroid studies in sheep pregnancy are complicated by the use of tocolytics to prevent premature labor, require technical experience with ultrasound guided fetal injections, and require a 100-120 day wait period to reach the appropriate gestational age for corticosteroid studies. We aspired to capture betamethasone release from the acetate prodrug and this objective can be easily accomplished by studying pharmacokinetics in the uncomplicated non-pregnant state. c) The dual acting formulation was evaluated as a single intramuscular injection of 0.5 mg/kg. This dose is higher than that recommended by the NIH in humans (0.17 mg/kg), but has been found to be the dosage in sheep that consistently produces preterm fetal lung maturation (Moss et al., 2001). This is also the highest dose level that can be investigated because it is associated with an injection size of 4-6 mL, which is the maximum recommended intramuscular administration volume (Rodger and King, 2000). The use of a high dose is necessary to capture the low-level betamethasone release that could occur from the acetate prodrug. The dose of the fast acting phosphate formulation was chosen to be 0.25 mg/kg. The 0.5 mg/kg injection of the dual formulation contains 0.25 mg/kg phosphate prodrug. Thus, betamethasone release by the acetate prodrug can be easily obtained by simple subtraction of the two profiles obtained from the two dose groups. d) We designed a liquid chromatography tandem mass spectrometry (LC/MS/MS) assay for measuring betamethasone that is capable of measuring low drug concentrations. This would help with the aim of measuring slow release of betamethasone from the acetate
prodrug. e) To overcome the problem of sample stability, plasma obtained from both formulation groups were stabilized using a 100 mM concentration of a phosphatase inhibitor sodium arsenate (Samtani et al., 2004b). In addition, samples from the dual prodrug group were stabilized with 86 mM potassium fluoride, which inhibits plasma esterases (Petersen et al., 1980).
Methods

Materials. Sodium arsenate heptahydrate, potassium fluoride, formic acid and prednisolone internal standard were purchased from Sigma-Aldrich (St. Louis, MO). The source for betamethasone was Steraloids Inc (Newport, RI). HPLC grade water and acetonitrile were from Burdick & Jackson (Muskegon, MI). Methanol was obtained from EMD Chemicals (Gibbstown, NJ). Phosphoric acid was from JT Baker (Phillipsburg, NJ) and ammonium formate was supplied by Fluka Biochemika (Buchs, Switzerland). Clinically used formulations for betamethasone phosphate (Celestan solubile) and betamethasone phosphate/acetate (Celestan depot) were from Essex Pharma in Munich, Germany.

Betamethasone Pharmacokinetic Study. Experimental procedures were approved by the Animal Care and Use Committee of the University of Wyoming, Laramie, WY. Eight Western Range ewes were weighed and brought into the animal facilities one day before the experiment. The animals were housed in outside pens and had ad libitum access to hay, hay cubes and water. On the day of the experiment, ewes were randomly assigned to two groups of four animals and were treated as follows. Group 1 received 0.25 mg kg⁻¹ betamethasone phosphate and the mean body weight of the animals in this group was 70 ± 6.4 kg (mean ± SD). Group 2 received 0.5 mg kg⁻¹ betamethasone phosphate / acetate mixture and the average body weight of the animals was 68 ± 9.4 kg. The injections were administered intramuscularly into the gluteal muscle at 8:30 AM in order to minimize the impact of circadian cortisol rhythms on the results. In both groups, blood samples were taken directly from the jugular vein at 15, 30, 45, 60, 90 min and at 3, 5, 8, 12, 24 h after each injection. In the dual formulation group,
additional blood samples were taken 2, 3, 4, 5, 6, 7, 8, 10, 12 and 14 days after the injection. Blood samples were collected in pre-chilled EDTA tubes and immediately put on ice after 50 µl of 2 M sodium arsinite solution per ml of blood was added for stabilization. After centrifugation, plasma was siphoned into plastic tubes and stored at –20°C. In the dual formulation group, 10 µl of 50% w/v potassium fluoride solution per ml of plasma was added to all the samples before freezing. Potassium fluoride was added to plasma and not to blood because addition of this stabilizer to blood causes lysis of red blood cells. Plasma samples were shipped on dry ice by overnight courier to Buffalo (State University of New York), where they were stored at –20°C until assayed by our LC/MS/MS method.

**Additional Data Source.** The maternal betamethasone profile after maternal intramuscular administration of 0.5 mg/kg phosphate/acetate formulation in pregnant sheep was obtained from a recently conducted meta-analysis (Samtani et al., 2004a).

**Sample Preparation.** Sample processing was carried out in lab plasticware to prevent the known adsorption of steroids to glassware (Makin et al., 1995). Non-specific adsorption can affect analyte sensitivity and recovery in the low-level analysis described in this work and the hydrophobicity of the polypropylene plastic surface helps reduce sample adsorption problems (Tsutsumi et al., 2003). Sample preparation involved adding 0.5 mL 4% phosphoric acid to 0.5 mL plasma sample in polypropylene tubes. This makes the samples less viscous and can free up the protein bound drug in plasma (Ding and Neue, 1999). 50 µL of a methanolic stock (1 µg/mL) of prednisolone was added as internal standard. After thorough mixing, samples were centrifuged at 8000g for 20 minutes and then subjected to solid phase extraction using Oasis HLB, 1 cc 30 mg
cartridges (Waters Corporation, Milford, MA). The extraction was carried out on a Vac Elut SPS 24 solid phase extraction manifold (Varian, Palo Alto, CA). The samples were extracted using the generic Oasis HLB procedure recommended by the manufacturer for 1 cc cartridges. Briefly, the SPE cartridge was pre-conditioned with 1 mL of methanol, followed by 1 mL of water. One ml of the processed sample was pulled through the cartridge, the cartridge was washed with 1 mL of 5% methanol in water and elution was performed with 1 mL methanol. The methanolic eluant was dried at 50°C under a gentle nitrogen stream and the dried residue was reconstituted with 50% 10 mM ammonium formate and 0.1% formic acid/50% acetonitrile. The reconstituted samples were transferred into 0.5 mL polypropylene tubes, centrifuged at 16000g for 10 min at 4°C and finally injected into the LC/MS/MS.

Plasma based standards and quality control (QC) standards were prepared from blank sheep plasma. Betamethasone methanolic stock solutions were added to polypropylene tubes and dried under nitrogen. Appropriate volumes of plasma were added, the tubes vortexed, and QC/standards were aliquoted at > 0.5 mL into 1.5 mL polypropylene tubes and stored at –20°C. The assay covers a concentration range of 0.1-100 ng/mL for betamethasone. Samples expected to have concentration greater than 100 ng/mL were diluted with an appropriate volume of blank plasma. Standards were run on a daily basis and samples and QC were quantified using a quadratic regression curve of analyte to internal standard area ratio vs. concentration with a weighting factor of 1/Y^2. The assay produced standard curves with r^2 ≥ 0.99, had an inter- and intra-assay accuracy and precision of ≤ 14%, and offered almost complete extraction recovery for betamethasone.
**LC/MS/MS Analysis.** Analysis was performed on a system equipped with an Agilent Technologies model 1100 autosampler (Palo Alto, CA), dual pump, and an Applied Biosystems PE/Sciex API 3000 mass spectrometer (Foster City, CA) using a turbo-ion spray source. The system control and data analysis were executed using the Analyst software (Applied Biosystems, Version 1.4). Chromatography was performed on a C₈ Hydrobond AQ column (particle size 3 uM, 2.1 x 150 mm, MAC-MOD Analytical Inc, Chadds Ford, PA) equipped with a ColumnSaver pre-column filter (MAC-MOD Analytical Inc). The mobile phase flow rate was 0.2 mL/min with eluant A consisting of 10 mM ammonium formate and 0.1% formic acid and eluant B consisting of acetonitrile. The mobile phase flow design was as follows: 0-4.5 min 40% A/60% B, 4.6-6.0 min: 10% A/90% B to allow system cleanup, followed by a 4 min equilibration step at 40% A/60% B. The mass spectrometer was operated in the positive ionization mode. The optimal ion pairs, declusturing potential, collision energy, collision exit potential, focusing potential, and excitation potential for betamethasone and prednisolone were found to be 393.3/373.3, 35V, 15V, 23V, 300V, 10V and 361.3/343.5, 25V, 15V, 20V, 300V, 10V, respectively. High purity nitrogen was used as the curtain and collision gas. The source temperature was set at 350°C.

**Pharmacokinetic Analysis.** Mean betamethasone concentration profiles as a function of time (t) after administration of the two formulations were fitted simultaneously using the models shown in Figure 1. The differential equations and their initial conditions used in the fitting procedure were as follows:

\[
\frac{dC_{\text{BMp}}}{dt} = \frac{ka_{\text{BMp}} \cdot \text{Dose}_{\text{BMp}} \cdot \exp\left(-k_{\text{disp}} \cdot t\right)}{V_c/F_{\text{BMp}}} - k_{\mu} \cdot C_{\text{BMp}}, \quad C_{\text{BMp}}(0) = 0 \quad (1)
\]

\[
\frac{dC_{\text{BMp/a}}}{dt} = \frac{ka_{\text{BMp}} \cdot \text{Dose}_{\text{BMp}} \cdot \exp\left(-k_{\text{disp}} \cdot t\right)}{V_c/F_{\text{BMp}}} + \frac{ka_{\text{BMa}} \cdot \text{Dose}_{\text{BMa}} \cdot \exp\left(-k_{\text{disp}} \cdot t\right)}{V_c/F_{\text{BMa}}} - k_{\mu} \cdot C_{\text{BMp/a}}, \quad C_{\text{BMp/a}}(0) = 0 \quad (2)
\]
where \(C_{BM_p}\) and \(C_{BM_p/a}\) refer to concentrations of betamethasone after administration of phosphate and phosphate/acetate formulations, \(k_{aBM_p}\) and \(k_{aBM_a}\) are hybrid first-order rate constants representing activation and absorption of betamethasone after intramuscular administration of phosphate and acetate prodrugs, \(Dose_{BM_p}\) and \(Dose_{BM_a}\) are the doses of phosphate and acetate prodrugs in terms of betamethasone equivalents, and \(V_c/F_{BM_p}\) and \(V_c/F_{BM_a}\) are the apparent volumes of distribution for betamethasone after administration of the betamethasone phosphate and acetate. Two different \(V_c/F\) terms are necessary because the two prodrugs may be activated to different extents in vivo. Finally, \(k_e\) is the elimination rate constant for betamethasone. Absorption and elimination half-lives were calculated as secondary parameters using the formula \(0.693/k\). Relative bioavailability (\(F_{BM_a}/F_{BM_p}\)) of the acetate vs. the phosphate prodrug was obtained from the ratio of the two apparent volumes of distribution. The pharmacokinetic modeling was performed using the maximum likelihood estimator within the ADAPT II computer program (D'Argenio and Schumitzky, 1997). The variance model was:

\[
\text{Variance} = \text{Coefficient} \cdot Y(t)^\text{Power}
\]

where Coefficient and Power are variance parameters that were fitted, and \(Y(t)\) represents the model output function. The goodness-of-fit was assessed using correlation coefficients, examination of residuals, and visual inspection.

**Extrapolation of Pharmacokinetic Profiles to Humans.** It will be shown later that the pharmacokinetics of betamethasone is not affected by pregnancy. Thus extrapolation of results from this study to the pharmacokinetic behavior of the two formulations in human pregnancy can be attempted. Allometric scaling is unnecessary because of the similarity in body weight of the ewes used in this study with humans. To
project human profiles, drug concentrations need to be scaled to the clinical dose and correction made for plasma protein binding to obtain free drug concentrations that drive corticosteroid effects. An estimate of possible fetal drug exposure can be obtained by recognizing that the placental barrier creates a fetal to maternal betamethasone concentration gradient in humans of approximately one-third (Samtani et al., 2004a). The correction factors needed to make human extrapolations are provided in Table 1. The calculations were performed in an Excel spreadsheet (Microsoft Excel software, Microsoft, Redmond, WA) by multiplying the combined correction factors with the appropriate predicted concentrations from the model fittings. To understand the relationship between projected concentrations and clinical outcome, efficacy and toxicity indices were calculated. Adrenal suppression was considered as a biomarker for assessing corticosteroid adverse effects. Prednisolone IC$_{50,\text{Free}}$ (free drug concentration causing 50% inhibition of cortisol synthesis rate) for adrenal suppression is known to be 1 ng/mL (Wald et al., 1992). Betamethasone, based on relative receptor affinity values, has a 3.6-fold higher affinity than prednisolone for the glucocorticoid receptor (Mollmann et al., 1995). Knowledge of the relative receptor affinities and prednisolone IC$_{50,\text{Free}}$ allows for calculation of a 0.3 ng/mL value for betamethasone IC$_{50,\text{Free}}$ (Mager and Jusko, 2002). Extrapolated maternal/fetal profiles for the two formulations were compared to this IC$_{50,\text{Free}}$ toxicity threshold to compare the two formulations. The longer the concentrations stay above the toxicity threshold, the greater is the potential for adverse effects.

The dissociation constant for the human fetal lung glucocorticoid receptor was chosen as an efficacy threshold. The evidence supporting corticosteroid mediated
induction of fetal lung maturation via the glucocorticoid cytosolic receptor and the utility of its dissociation constant have been reviewed (Ballard and Ballard, 1995). Most data comes from experiments performed with fetal lung explant cultures. Fetal lung cells have been shown to possess glucocorticoid receptors and the effects seen with glucocorticoids are reversible indicating reversible binding of steroids to their receptors. Induction experiments show considerable delay in peak effects, (24 and 48 hr for mRNA and protein up-regulation) which is in accordance with transcription and translation delays that occur after receptor binding. Induction effects have been observed only upon exposure to glucocorticoids and not when cells were treated with androgens, estrogens or progestins. Most importantly, half-maximal induction of various molecular markers of fetal lung maturation occurs at concentrations that are similar to the dissociation constant values for receptor binding of glucocorticoids. We therefore chose the dissociation constant for the human fetal lung glucocorticoid receptor as the efficacy threshold. A dissociation constant of 5 nM for dexamethasone is available in the literature (Gonzales et al., 1986). Dexamethasone has 1.7-fold higher affinity than betamethasone for binding to the glucocorticoid receptor in the human lung (Mollmann et al., 1995). This information allows calculation of a dissociation constant value of 8.5 nM (3 ng/mL) for betamethasone. Extrapolated maternal/fetal profiles for the two formulations were compared to this efficacy threshold to discern which of the two formulations may have a better efficacy profile. The longer the concentrations stay above the efficacy threshold, the greater is the potential for producing fetal lung maturation. Extrapolated free betamethasone concentrations in fetal plasma can be directly compared to the
dissociation constant for the receptor residing intracellularly in the lung because the lipophilicity of the steroid allows ready passage across cellular membranes.
Results

**LC/MS/MS Analysis for Betamethasone.** The enhanced sensitivity of the LC/MS/MS assay and the high doses used in the study allowed characterization of betamethasone pharmacokinetics for 24 hours for the phosphate and for 5 days for the phosphate/acetate formulations (Figure 2). The assay was adapted from a method described for rat plasma samples (Tamvakopoulos et al., 2002). An important change was made wherein the assay was scaled up to make it suitable for plasma samples from sheep. Tamvakopoulos et al. measured betamethasone in small volume rat plasma samples and hence used a 96-well miniaturized HLB Oasis extraction format. Sample volume was not a limitation in our study and we wished to measure extremely low drug concentrations. We therefore used the HLB Oasis cartridge format for extracting plasma samples which involved a ten-fold larger sample volume (500 vs. 50 µL). By using a larger sample volume we were able to reduce the assay lower limit of quantification of 2 ng/mL reported by Tamvakopoulos et al. to 0.1 ng/mL. During the preparation of this manuscript two other methods describing LC/MS/MS analysis of betamethasone in plasma were published (Taylor et al., 2004; Luo et al., 2005). These methods monitor different daughter ions in tandem MS for betamethasone and make use of longer liquid-liquid extraction based sample preparation methods. However, both these methods are similar to our assay in terms of assay sensitivity, accuracy, precision, specificity and quantifiable concentration range.

**Betamethasone Pharmacokinetic Profiles.** The mean betamethasone concentration profiles produced by the two formulations and the fitted curves are shown in Figure 2. The profiles reported here, unlike all the sheep profiles summarized in a
recent meta-analysis (Samtani et al., 2004a), show a distinct absorption/formation phase. The latter is indicative of lack of sample instability artifacts, which were prevented by addition of enzyme inhibitors. Both formulations produced a peak concentration of about 180 ng/mL at 1-1.5 hour, which reflects the fast input from the phosphate prodrug (Table 2: $k_\text{aBMp}$ half-life of 0.3 hr). Whereas the phosphate formulation profile appeared like a traditional Bateman function with a terminal half-life of 4 hours, the phosphate/acetate formulation produced a biexponential decline with a shallow terminal half-life of 14 hours. The betamethasone profile emerging from the acetate prodrug was obtained by simple subtraction of the two fitted curves and is depicted in Figure 2. The longer terminal half-life of the dual prodrug formulation can be attributed to flip-flop kinetics where the slow decline in concentrations is reflective of the delayed sustained-release of betamethasone from the intramuscular site. The lack of a distribution phase in the phosphate formulation profile suggests that the distribution process for betamethasone is either rapid or obscured by the formation/absorption phase. This pattern justifies the one-compartment model depicted for betamethasone in Figure 1. The model fitted curves in Figure 2 indicate that the proposed models well captured the betamethasone pharmacokinetics. The estimated pharmacokinetic parameters are listed in Table 2 and the < 15% coefficient of variation for all fitted parameters is indicative of excellent model performance.

**Effect of Pregnancy on Betamethasone Pharmacokinetics.** Figure 3 shows the fitted pharmacokinetic profile for the 0.5 mg/kg dual formulation from this study superimposed over the data from a recent meta-analysis depicting maternal pharmacokinetics from pregnant sheep at the same dose level. There is a lack of
agreement at the early time points between the two datasets, which can be attributed to lack of sample stabilization in the pregnant animal data. Apart from the early disconnect in concentrations, there is reasonable agreement between the two datasets. This pharmacokinetic trait of similarity in betamethasone disposition between the pregnant and non-pregnant states has also been observed in humans (Benet et al., 1996). We have recently shown that sheep pharmacokinetic profiles for betamethasone in pregnant sheep are a good representation of human profiles in pregnancy (Samtani et al., 2004a). Minimal scaling of pharmacokinetics is required because of similarity in body weights. The resemblance between humans and sheep for betamethasone pharmacokinetics during the pregnant and non-pregnant states allows the use of sheep as excellent animal model for anticipating betamethasone disposition during pregnancy in humans.

**Extrapolated Human Profiles.** Extrapolations to the human situation are shown in Figure 4 and they indicate that the two formulations given at equal doses will produce markedly different profiles in the maternal and fetal circulations. The 12 mg dose of betamethasone in the form of the phosphate prodrug would generate higher peak levels both in the mother and the fetus and produce a steep decline in concentrations. In contrast 12 mg of the dual formulation (8 mg betamethasone phosphate equivalent to 6 mg betamethasone and 6 mg betamethasone acetate) would produce lower peak concentrations in the maternal and fetal circulations. However, maternal and fetal profiles would have a prolonged terminal half-life because of the sustained-release nature of the acetate prodrug.

The delayed release property of the dual formulation causes betamethasone concentrations to stay above the proposed toxicity threshold for a longer period in
maternal and fetal plasma and this sustained exposure is shorter in the fetal than in the maternal circulation. This is because restricted placental access of betamethasone produces lower peak concentrations in the fetus and hence it takes a shorter duration of time for betamethasone levels to fall below the toxicity threshold.

Finally, the time of exposure to therapeutic betamethasone concentrations in the fetal circulation is similar. Both formulations produce profiles that cross the therapeutic threshold at approximately the same time.
Discussion

**Choice of LC/MS/MS for Analysis.** Commonly used HPLC assays for corticosteroids have a lower limit of quantitation of 10 ng/mL (Jusko et al., 1994). Other methods based on gas chromatography/mass spectrometry and fluorescence detection, although offering highly specific and sensitive analysis, require derivatization (Frerichs and Tornatore, 2004). Bioanalytical methods based on LC/MS/MS represent the most specific and sensitive methods for steroid analysis (Lai et al., 2002). This technique coupled with solid phase extraction combines the attributes of rapidity, easy processing, accuracy, specificity, sensitivity and precision without the need for sample derivatization. We therefore assayed betamethasone in sheep plasma using a solid phase extraction LC/MS/MS method, which allowed measurement of slow betamethasone release from the acetate prodrug.

**Release Rates of Active Steroid by Betamethasone Prodrugs.** It is generally accepted that the conversion of the acetate and phosphate prodrugs to the active corticosteroid is a relatively fast process. Studies in rodents have shown that the acetate prodrug administered intravenously (dissolved in dimethylsulfoxide containing saline) produces corticosteroid pharmacokinetics that are identical to those produced by an intravenously administered phosphate prodrug (Ogiso et al., 1987). The inability of the conversion process to serve as a rate-limiting step is not surprising because activating enzymes such as phosphatases and esterases are highly efficient and ubiquitous (Krise et al., 1999).

The release rate of betamethasone from the two prodrugs is controlled by their physicochemical properties. The phosphate prodrug being highly ionized has an aqueous
solubility of 625 mg/mL (Harvey, 1975). It is injected as a solution and exhibits rapid absorption after intramuscular administration. Consequently, the disposition processes controlling betamethasone pharmacokinetics dictate the terminal decline in concentrations after injection of the phosphate prodrug. In contrast, the acetate prodrug is highly hydrophobic, has an aqueous solubility of 30 µg/mL (Kabasakalian et al., 1966), and is administered intramuscularly as a suspension. The > 20000-fold lower solubility creates dissolution rate limited absorption of the acetate prodrug. It has to first dissolve in the fluids of the intercellular space of muscle fibers before it can diffuse into the vascular space (Hirano et al., 1981). For practically water insoluble molecules in vitro solubility is directly correlated to in vivo absorption after intramuscular injection of an aqueous suspension (Zuidema et al., 1994). The solubilization of the suspension is often the slowest event amongst the ADME processes after intramuscular injection. The rate limiting solubilization process is reflected in the terminal slope of the pharmacokinetic profile leading to flip-flop kinetics. Furthermore, inter-species differences in the terminal half-life are not expected since the dissolution process at the injection depot governs the terminal decline (Zuidema et al., 1994). Thus the long half-life observed for betamethasone in this study after injection of the dual formulation may also occur in humans. We believe that the long half-life has not been detected previously after intramuscular administration because of assay and sampling limitations. Furthermore, the acetate prodrug is also only 62% bioavailable as compared to the phosphate prodrug (Table 2: \( F_{\text{BMa}}/F_{\text{BMP}} = 62.3\% \)). This is not surprising because highly lipophilic compounds produce biphasic absorption after intramuscular injection, where the second slow phase is exceptionally difficult to capture leading to the conclusion of incomplete
bioavailability (Zuidema et al., 1994). This slow second phase is thought to produce a “hang-over effect”, which leads to drug levels that are probably not therapeutically useful and may be a source of unwanted side effects (Zuidema et al., 1994). The possibility even exists that some drug continues to be absorbed beyond 120 hr with a third phase of release (Figure 2).

**Biexponential Decline Following the Dual Formulation.** Multiexponential decline patterns for betamethasone can be observed due to various reasons. Possibilities include: i) Spurious overestimation of concentrations due to sample instability (Samtani et al., 2004b), ii) Tissue distribution, iii) Dual betamethasone input. It is often assumed that the acetate prodrug does not release betamethasone and the biexponential profile has been attributed to tissue distribution (Samtani et al., 2004a). However, Figure 2 clearly indicates that the acetate does have sustained-release properties and the phosphate prodrug profile lacks an obvious distribution phase. Furthermore, we prevented artifactual overestimation of concentrations by sample stabilization and therefore the most probable explanation for betamethasone multiexponentiality is dual steroid input. This probably indicates that estimates of tissue distribution volumes and clearances reported in the literature need to be interpreted with caution because they may have been estimated inaccurately due to model misspecification.

Observation of a biexponential decline pattern is a typical feature of analytes with dual input. A classic example is metabolite kinetics observed after oral administration of a drug exhibiting high oral first-pass effect (Rowland and Tozer, 1995). The mathematical rationale behind the biexponential decline can be readily understood by
analyzing equation 2 for the dual formulation. Integrating equation 2 gives the following explicit equation:

$$C_{BMp} = \frac{ka_{BMp} \cdot \text{Dose}_{BMp}}{V_c/F_{BMp}(k_d - ka_{BMp})} (\exp^{-ka_{BMa} \cdot t} - \exp^{-k_d \cdot t}) + \frac{ka_{BMa} \cdot \text{Dose}_{BMa}}{V_c/F_{BMa}(k_d - ka_{BMa})} (\exp^{-ka_{BMa} \cdot t} - \exp^{-k_d \cdot t}) \quad (4)$$

The explicit equation is merely a sum of two Bateman functions where one function has $k_d$ as the rate-limiting process, while the other has $ka_{BMa}$ as the rate-limiting step. The two functions are displaced in time because of different rate-limiting processes and superimposition of two such functions produces a curve with biexponential decline.

**Reconciling Different Beliefs about Acetate Prodrug Release.** Studies that have concluded that the acetate prodrug does not release betamethasone were short duration studies that spanned 8-10 hours (Petersen et al., 1984). Figure 2 demonstrates that during this early time period the pharmacokinetic profiles from the two formulations are virtually super-imposable. Due to the depot release nature of the acetate prodrug, it delivers very little betamethasone during this early period. The minuscule amount of betamethasone released during the early phase and the inability to measure the low concentrations of betamethasone beyond of 8-10 hours has led to erroneous conclusions about the acetate prodrug. In contrast, studies conducted by Ballard et al. have examined the clinical dosing regimen of two doses of 12 mg betamethasone phosphate/acetate 24 hours apart (Ballard et al., 1975). Based on the half-life obtained from this study and information from betamethasone phosphate studies in non-pregnant subjects Ballard has stated that the dual formulation does have sustained-release properties (Ballard, 1986; Ballard and Ballard, 1995). The terminal half-life of 6 hours reported by Ballard is the widely accepted half-life for betamethasone after administration of the dual formulation (Dudley et al., 2003, Padbury et al., 1996). Although, Ballard made an insightful and
accurate conclusion about the dual release properties of the phosphate/acetate formulation, the commonly accepted half-life is probably incorrect. Based on the data in Figure 2, it is obvious that the true terminal decline phase of betamethasone from the acetate prodrug will be missed if the profile is followed for any duration less than 2-3 days. In light of this new finding, dosing recommendations for betamethasone formulations need to be reassessed. This finding is particularly important because in the United States, the only injectable form of betamethasone recommended and available for antenatal use is the dual formulation. Betamethasone sodium phosphate injection now appears in the “discontinued” section of FDA’s Orange Book because Schering-Plough discontinued the manufacture of this product in May 2002. Furthermore, many clinicians have adopted the practice of giving multiple doses (as many as 11 repeat courses) of betamethasone to enhance fetal lung maturation (Andrews and Matthews, 2003). The prolonged half-life for betamethasone from the intramuscular depot combined with multiple-dosing can have accumulative and unfavorable effects in the mother and fetus and this will be discussed below.

**Implications of a Prolonged Half-Life on Fetal and Maternal Health.** Results from Figure 4 indicate that both formulations produce similar early exposures, but the dual formulation could have a lower safety index. This is supported by the fact that efficacy of both formulations has been demonstrated in pregnancy trials. However, a recently conducted meta-analysis (Jobe and Soll, 2004) has shown that betamethasone use in pregnancy might be associated with a higher incidence of maternal infections as compared to dexamethasone. The majority of the betamethasone trials in the meta-analysis used the dual formulation, whereas dexamethasone was exclusively used as the
phosphate prodrug. The mother serves as a delivery mode and reservoir for the steroid and is exposed to betamethasone levels three times higher than the fetus. The practice of exposing the parturient mother to steroid levels that are of no therapeutic benefit to her and probably lead to adverse effects is unfortunate. Reassessment of use of this dual formulation regimen during pregnancy is warranted.

Several assumptions have been made in arriving at the conclusion regarding the reassessment of corticosteroid dosing regimens during pregnancy. These conclusions need to be supported by additional long duration experimental data on corticosteroid pharmacokinetics, adrenal suppression, and fetal drug exposure from different formulations during pregnancy. Corticosteroids have been used for precocious induction of fetal lung maturation for over thirty years. However, the pharmacokinetic, pharmacodynamic and toxicodynamic properties of corticosteroids in pregnancy are poorly understood and can be improved by well-designed mechanistic studies using modern analytical tools.
DMD #4309

Acknowledgements

We thank Donna Ruszaj for helpful discussions and technical assistance with LC/MS/MS assay development.
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Footnotes

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Legends for figures

Figure 1. Pharmacokinetic models for characterizing the time course of betamethasone concentrations after (A) Intramuscular dosing of 0.25 mg/kg betamethasone phosphate and (B) Intramuscular dosing of 0.5 mg/kg betamethasone phosphate/acetate dual formulation.

Figure 2. Results of the pharmacokinetic study with data points and standard deviation bars representing mean betamethasone concentrations in plasma from four animals after administration of betamethasone phosphate (▲) and the dual formulation (●). Solid and dashed curves are profiles fitted simultaneously to the phosphate and dual formulation data. The dotted curve represents the deduced betamethasone profile arising from the acetate component of the dual formulation. Inset: Betamethasone concentrations and fitted curves on a linear scale for the first five hours.

Figure 3. The fitted pharmacokinetic profile for the 0.5 mg/kg dual formulation profile from Figure 2 superimposed over data from a recent meta-analysis (Samtani et al., 2004a) depicting maternal betamethasone pharmacokinetics from pregnant sheep over 24 hr at the same dose level.

Figure 4. Extrapolated human profiles for unbound (A) maternal and (B) fetal betamethasone concentrations. Solid and dashed curves represent profiles for the dual and phosphate formulations. Horizontal lines depict the toxicity threshold (solid circles) and the efficacy threshold (open circles).
Table 1. Correction factors needed to make human extrapolations

<table>
<thead>
<tr>
<th></th>
<th>Scaling to the clinical dose</th>
<th>Fetal to maternal gradient</th>
<th>Plasma free fraction</th>
<th>Combined correction factor</th>
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<tbody>
<tr>
<td><strong>Maternal Circulation</strong></td>
<td></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>Phosphate/acetate formulation</td>
<td>0.34&lt;sup&gt;a&lt;/sup&gt;</td>
<td>N/A</td>
<td>0.4&lt;sup&gt;b&lt;/sup&gt;</td>
<td>0.14</td>
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<tr>
<td>Phosphate formulation</td>
<td>0.68&lt;sup&gt;c&lt;/sup&gt;</td>
<td>N/A</td>
<td>0.4&lt;sup&gt;b&lt;/sup&gt;</td>
<td>0.28</td>
</tr>
<tr>
<td><strong>Fetal Circulation</strong></td>
<td></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>Phosphate/acetate formulation</td>
<td>0.34&lt;sup&gt;a&lt;/sup&gt;</td>
<td>0.28&lt;sup&gt;d&lt;/sup&gt;</td>
<td>0.59&lt;sup&gt;b&lt;/sup&gt;</td>
<td>0.06</td>
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<tr>
<td>Phosphate formulation</td>
<td>0.68&lt;sup&gt;c&lt;/sup&gt;</td>
<td>0.28&lt;sup&gt;d&lt;/sup&gt;</td>
<td>0.59&lt;sup&gt;b&lt;/sup&gt;</td>
<td>0.11</td>
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</tbody>
</table>

<sup>a</sup> Ratio of the clinical dose (0.17 mg/kg) to the studied dose (0.5 mg/kg)

<sup>b</sup> Petersen et al., 1983

<sup>c</sup> Ratio of the clinical dose (0.17 mg/kg) to the studied dose (0.25 mg/kg)

<sup>d</sup> Samtani et al., 2004a
Table 2. Estimated betamethasone pharmacokinetic parameters after administration of two prodrug formulations

<table>
<thead>
<tr>
<th>Parameter</th>
<th>Estimate</th>
<th>CV (%)&lt;sup&gt;a&lt;/sup&gt;</th>
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<tbody>
<tr>
<td>$k_{a_{BM_p}}$ (1/day)</td>
<td>60.6</td>
<td>9.19</td>
</tr>
<tr>
<td>$k_{a_{BM_a}}$ (1/day)</td>
<td>1.25</td>
<td>5.36</td>
</tr>
<tr>
<td>$V_c/F_{BM_p}$ (L/kg)</td>
<td>1.10</td>
<td>3.57</td>
</tr>
<tr>
<td>$V_c/F_{BM_a}$ (L/kg)</td>
<td>1.77</td>
<td>12.2</td>
</tr>
<tr>
<td>$k_{el}$ (1/day)</td>
<td>4.21</td>
<td>3.72</td>
</tr>
<tr>
<td>$t_{1/2}$ $k_{a_{BM_p}}$ (hr)</td>
<td>0.275&lt;sup&gt;b&lt;/sup&gt;</td>
<td>9.19</td>
</tr>
<tr>
<td>$t_{1/2}$ $k_{a_{BM_a}}$ (hr)</td>
<td>13.3&lt;sup&gt;b&lt;/sup&gt;</td>
<td>5.36</td>
</tr>
<tr>
<td>$t_{1/2}$ $k_{el}$ (hr)</td>
<td>3.95&lt;sup&gt;b&lt;/sup&gt;</td>
<td>3.72</td>
</tr>
<tr>
<td>$% F_{BM_a}/F_{BM_p}$</td>
<td>62.3&lt;sup&gt;b&lt;/sup&gt;</td>
<td>12.1</td>
</tr>
</tbody>
</table>

<sup>a</sup>Coefficient of variation of the estimate, not reflective of inter-animal variability

<sup>b</sup>Secondary parameters
Fig. 1
Fig. 2
Fig. 3
Fig. 4